VLSI Implementation of a Conductance-based Multi-Synapse using Switched-Capacitor Circuits

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Abstract—For neuromorphic ICs, the implemented synaptic dynamics play an important role in the complexity achievable when running networks on the overall IC. One of these ingredients for realistic dynamics are conductance-based synapses, which in contrast to current-based synapses let a neuron adapt in various ways to its input characteristics. Another ingredient is classical neuronal spike-frequency adaptation. Both are usually realized in fully-analog subthreshold circuits, making them hard to port to modern sub-100nm technologies. In contrast, we present a compact switched-capacitor (SC) model of a conductancebased synapse that can be widely configured to accurately depict e.g. NMDA, GABA or AMPA type synapses. The SC approach is inherently easy to port between technologies and its digital part benefits fully from technology scaling. We show how this synapse circuit can also be utilized to endow a neuron with spikefrequency adaptation (SFA).

Keywords—conductance-based, multi-synapse, spike-frequency adaptation, switched-capacitor, neuromorphic

I. INTRODUCTION

In order to support the advancing knowledge in the field of neuroscience, state-of-the-art neuromorphic circuits must provide biologically realistic behavior, incorporating e.g. conductance-based synapses [1], exponentially decaying conductance trace and dynamic behavior such as SFA and voltage dependent synaptic responses (e.g. NMDA-type synapses). Most analog implementations of neuromorphic circuits rely on so-called subthreshold circuits. These are hard to port to small CMOS techologies, since leakage currents rapidly increase with down-scaling, reaching the range of the desired signal currents. Additionally, device mismatch and process variation increase and the range of transistor transfer functions usable for computation is very limited. This is why even recent neuromorphic systems have been manufactured in quite large technologies [2]-[4]. Furthermore, significant deviations caused by device mismatch and process variation have to be expected even there, so control voltages have to be adjusted very accurately. On the other hand, due to relatively high current ranges analog neuromorphic circuits exploiting MOS transistors in saturation [5] mostly suffer from realtime capability, which is important for e.g. interfacing living nerve tissue and processing real-world input stimuli. These problems can be largely circumvented by using SC circuits [6], [7], which utilize robust charge-based signal transmission and offer a wide-range configurability. Due to the mixedsignal approach with a relatively large digital circuitry for controlling the analog circuit, they can be ported easily to small technologies, since only standard building blocks like opamps, switches and capacitors are required. This again allows a high



Fig. 1. Leaky integrate-and-fire neuron with different types of conductancebased multi-synapses and spike-frequency adaptation.

accuracy of the reproduction of biologically realistic behavior [8].

In this paper we present a mixed-signal neuromorphic system with SC synapses and a digital circuitry calculating the conductance value of high input count multi-synapses, consisting of standard analog building blocks and synthesizable digital logic. We describe circuit techniques to reduce leakage currents for achieving higher time constants. Additionally, we present an approximation to the nonlinear voltage dependence of NMDA synapses that simplifies circuit implementation, while closely matching the exact formulation in the relevant voltage range.

II. CIRCUIT DESCRIPTION

The circuit models a leaky integrate-and-fire neuron [9] with SFA and several types of conductance based multisynapses (see Fig. 1). The synaptic current of each type is

$$I_{syn,i} = g_{syn,i} (E_{syn,i} - V_m), \qquad (1)$$

with membrane voltage V_m , reversal potential $E_{syn,i}$ and the synaptic conductance $g_{syn,i}$ modeled by

$$\frac{\mathrm{d}g_{syn,i}}{\mathrm{d}t} = \frac{-g_{syn,i}}{\tau_{syn,i}} + \Delta g_{syn,i} \sum_{k} w_k \delta(t - t_k) \,. \tag{2}$$

This results in an exponentially decaying conductance with the corresponding time constant τ_{syn} and with instantaneous increments depending on a global conductance change $\Delta_{g_{syn,i}}$ and a specific weight w_k at each incoming spike k at time t_k . Since different weights can be applied for each spike and the resulting conductance changes sum linearly on one variable this synapse can emulate an arbitrary number of individual synapses [1], hence the name "multi-synapse".

The circuit of the conductance-based multi-synapse makes use of a mixed signal approach, where the time-varying conductance value is stored and computed in a digital sub-circuit



Fig. 2. Principle schematic of the leaky integrator circuit emulating the synaptic conductance.

(see grey box in Fig. 1) and the membrane capacitance of the postsynaptic neuron as well as the synaptic conductance itself are represented by analog circuitry. The circuit offers several simultaneously acting synapse types, which can be configured individually for e.g. NMDA-, GABA- or AMPA-type behavior. The adjustment includes time constant, amount of conductance change at incoming spikes and the corresponding reversal potential.

A. Switched-Capacitor Synapses

Fig. 2 shows the principle of operation for conductancebased synapses using SC circuits. In contrast to the circuit in [6], the membrane voltage is buffered by an opamp for further computation in the NMDA circuit (described in Sec. II-E) and for monitoring. The synaptic conductance is modeled by an SC resistor emulation, consisting of C_{syn} and switches S_1 to S_4 . In combination with the parallel membrane capacitor, a leaky integrator is created. S_1 , S_2 and S_3 , S_4 , respectively, are switched alternately and non-overlapping as indicated by switch phases Φ_1 and Φ_2 . In phase Φ_1 capacitor C_{syn} is precharged by the synaptic reversal potential E_{syn} , and in Φ_2 a charge equalization on C_{syn} and C_m occurs. The conductance value is determined by the switching frequency f_{switch} and the capacitance C_{syn} :

$$g_{syn} = C_{syn} \cdot f_{switch} \tag{3}$$

The analog circuit realizing the leaky-integrate-and-fire neuron with multiple synapse types is shown in Fig. 3. Its fully-differential architecture has been chosen to reduce charge injection and clock feedthrough. A simple SC common-mode feedback network (not shown) controls the common-mode voltage $V_{cm} = V_{DD}/2$. The SC resistor emulators representing the synaptic conductances are connected in parallel to the membrane capacitor. An on-chip 8 bit digital-to-analog converter provides the different reversal potentials for the corresponding synapse types.

B. Leakage Current Reduction

A major issue in SC circuits is leakage current through switches, particularly when moving to sub-100nm technologies. Especially for neuromorphic circuits with time constants in the milliseconds range, low switching frequencies and small capacitance values, these currents have a strong impact on the accuracy of model reproduction. A way to reduce these effects is by applying low-leakage switches as shown in [10], where



Fig. 3. SC neuron circuit with conductance-based synapses and comparator for threshold detection.

a MOS switch is split into two transistors and the middle node voltage is drawn to V_{DD} in off-state (see upper right of Fig. 3). Simulations have shown that leakage can be further reduced by choosing a voltage between V_{DD} and ground. In Fig. 3 this method has been applied with switches S1 - S6. S2 and S3 disconnect C_m from the opamp feedback loop. S1 and S4 set the outer nodes of the switches to a defined voltage which is equal to V_{cm} in this case. This reduces subthreshold currents through MOS transistors of S2 and S3 since V_{DS} is kept low. Furthermore, subthreshold leakage currents are kept independent of the opamp output voltage. Another advantage of the proposed switch configuration is the absence of gate leakage at the opamp input which otherwise would draw current from the membrane capacitor. A reduction of junction leakage at the switches surrounding C_m can be achieved by minimally sized drain and source areas. In order to effectively exploit this low leakage technique, the membrane capacitor is decoupled from the circuit whenever none of the synapse, SFA or leakage generation circuits is in its second switch phase Φ_2 , where C_{syn} is connected to C_m . In this state S5 and S6 disconnect the opamp from the rest of the circuit and S7 closes a negative feedback loop around the opamp, which prevents the opamp outputs from floating towards supply rails.

C. Digital Generation of the Conductance Trace

Eq. (2) is implemented by the digital circuit shown in Fig. 4. Its main parts are the conductance trace generation and a numerical-to-frequency conversion, which triggers the switch event generation for the SC circuit. The conductance trace generation sub-circuit holds a register GSYN REG, which stores the conductance value. If a spike arrives, meaning VALID is high for one clock cycle, the weight of this spike is added to GSYN_REG. Between incoming spikes the conductance value decays exponentially towards zero. This is done by subtracting the value of GSYN_REG shifted right by 6 bit, which results in a multiplication by $1-2^{-6}=0.984375$, in a constant interval configured by TAU_SYN. TAU_COUNTER is incremented at each system clock cycle and when it reaches TAU_SYN it is reset and the subtraction is done. This leads to a direct proportionality between the synaptic time constant and the configuration value $\tau_{syn} = -TAU_SYN/(f_{clk} \cdot \log(1-2^{-6})).$



Fig. 4. Block diagram of the digital circuitry.

In the second part, the conductance is accumulated on the phase register PHASE_REG, which is clocked analogously to GSYN_REG. When an overflow is detected by the adder the two switch phases for the analog part of the synapse are triggered. With this method, the value of GSYN_REG is converted linearly to the switching frequency. Scaling of the frequency can be done with DELTA_GSYN, which is inversely proportional to the conductance change $\Delta g_{syn,i}$ in Eq. (2).

D. Modeling SFA with Conductance-based Multi-synapses

A phenomenon especially present in pyramidal cells is SFA. As shown in [9], it can be modeled in a similar way as the conductance of a multi-synapse with a certain reversal potential E_{sfa} , where g_{sfa} tends to shunt the membrane capacitance dependent on the spiking frequency of the neuron, which decreases the neuron's excitability. For this, a fixed amount is added to g_{sfa} at each post-synaptic spike. In our implementation, the same synapse circuit can be used for SFA with only minor modifications. The spike output of the neuron has to be connected to the spike input of the SFA circuit and the WEIGHT signal can be set to a fixed value, e.g. 1.

E. Modeling NMDA-Type Synapses

In contrast to other synapse types, NMDA synapses show a dependence between conductance value and membrane potential [9]. The synaptic current of NMDA-type synapses can be modeled by

$$I_{nmda} = g_{nmda0} \frac{(E_{nmda} - V_m)}{1 + 0.28 \cdot \exp(\frac{V_m}{16.129 \,\mathrm{mV}})}, \qquad (4)$$

with $E_{nmda} = 0$. The nonlinear dependence of the conductance on V_m is difficult to faithfully reproduce in a circuit implementation. As can be seen in Fig. 5, this dependence can be well approximated linearly in the range between lowest reversal potential at about $-70 \,\mathrm{mV}$ for inhibitory synapses and threshold voltage at about $-50 \,\mathrm{mV}$:

$$I_{nmda}^*/g_{nmda0} = \alpha (V_m - E_{nmda}^*).$$
⁽⁵⁾

We can rewrite Eq. (5) to get a regular conductance-based synapse $I_{nmda}^* = g_{nmda0} \cdot (E_x - V_m)$, with a voltage-dependent reversal potential

$$E_x = V_m + \alpha (V_m - E_{nmda}^*).$$
(6)



Fig. 5. Linear approximation of the voltage dependence of NMDA-type synapses.



Fig. 6. SC circuit providing the membrane voltage dependent reversal potential for NMDA synapses.

The circuit generating the voltage-dependent reversal potential is depicted in Fig. 6. In the sampling phase Φ_1 , the membrane potential is stored on the binary weighted capacitors C1-C3 corresponding to α , and on C4, whereas C5 is reset. In Φ_2 , the fraction α of $V_m - E^*_{nmda}$ is integrated on C5 and the output voltage is shifted by V_m , resulting in an output voltage as described in Eq. (6).

III. RESULTS

The neuromorphic system was designed in a 180 nm CMOS technology with a supply voltage of 1.8 V. A neuron circuit including one NMDA circuit has a power consumption of $45\,\mu\text{W}$ and a total silicon area of $18\,000\,\mu\text{m}^2$. The digital circuit consumes an area of $45\,000\,\mu\text{m}^2$ for one neuron with 5 synapse types and has a power consumption of approximately 100 µW. Sources of deviations from the ideal model parameters are opamp non-idealities, capacitor mismatch and leakage currents. Due to the differential voltage swing of 1.5 V, the opamp offset voltage of less than 10 mV is negligible. Capacitor mismatch has an effect on the membrane time constant and conductance values of the synapses, but can be compensated by digital configuration. Unfortunately, we are not provided with Monte-Carlo simulation models for the MIM capacitors we used, so only a nominal simulation has been carried out. Simulation results are depicted in Fig 7. The upper diagram shows the membrane voltage trace V_m . At 1 ms, the neuron is stimulated with a 10 kHz spike train for 10 ms arriving at an AMPA synapse with high reversal



Fig. 7. Simulation results of membrane potential with synaptic input from three different synapse types.

potential and $\tau_{ampa} = 2 \text{ ms.}$ At 30 ms, an inhibitory GABA spike is triggered ($\tau_{gaba} = 10 \text{ ms}$), which decreases the membrane potential. From 40 ms to 70 ms, a 1 kHz spike train arrives at the NMDA synapse ($\tau_{nmda} = 100 \text{ ms}$). The supra-linear increase of the membrane potential indicates the voltage dependence of NMDA-type synapses (see Eq. (6)). After reaching the threshold voltage at about 90 ms the neuron fires and is reset to its reset voltage.

Our implementation focuses on a robust reproduction of the model equations and a high number of synaptic inputs, which are required e.g. when simulating population bursts [11]. Other implementations of conductance-based synapses may consume less area, but at the cost of reduced functionality and robustness. A subthreshold circuit of a conductance-based synapse with NMDA behavior is presented in [2]. The synapse circuit was designed in a $0.35\,\mu\text{m}$ process and consumes an area of $1360\,\mu\text{m}^2$. While this circuit was designed as a single synapse, it could be used as multi-synapse as well, by discarding the short-term plasticity mechanism. However, it is not able to support such a high input count as our implementation. Furthermore, due to the exponential dependence between control voltage and current signals, synaptic behavior is very sensitive to device mismatch and process variation.

Another implementation of a conductance-based multisynapse using SC circuits can be found in [6]. It was fabricated in a $0.5 \,\mu\text{m}$ process where a neuron circuit with one multisynapse consumes an area of about $3700 \,\mu\text{m}^2$. Here each incoming pulse event triggers a switch event, which transmits a charge packet. Although this is a very flexible approach, exponentially decaying conductance traces and summation over synapses have to be generated off-chip. In contrast, these features are an important part of our integrated implementation.

As an outlook, memristive technologies could profit from our circuit principle: By connecting the memristor terminals to the postsynaptic membrane and a pulsed voltage source driven by the switch event generation circuit, learning memristive arrays [12] could be equipped with conductance-based synapses.

IV. CONCLUSION

We presented a conductance-based high input count multisynapse using SC circuits. With a slight modification, the circuit can be used to model SFA. Furthermore, it has been shown how the voltage dependent behavior of NMDA-type synapses can be implemented with additional circuitry. The overall silicon area of the neuron is $63\,000\,\mu\text{m}^2$ and consumes less than 100 µW of power. Due to a large capacitance array consisting of unity capacitors of $50 \,\mathrm{fF}$ ($100 \,\mathrm{\mu m^2}$), a fullydifferential architecture and a dedicated low-leakage technique, a high model accuracy is achieved compared to existing subthreshold circuits [2] and SC implementations [6]. Since the area is strongly dominated by MIM capacitors, it could be shrunk with relaxing the accuracy requirements. The large digital part would perfectly benefit from technology scaling. In contrast to [6], our circuit is equipped with exponentially decaying conductances and is designed to emulate up to 10k synaptic inputs at a firing rate of 10 Hz providing a biologically realistic behavior.

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